

State-of-Art IMPT vs. IMRT

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Chicago, April 27, 2013



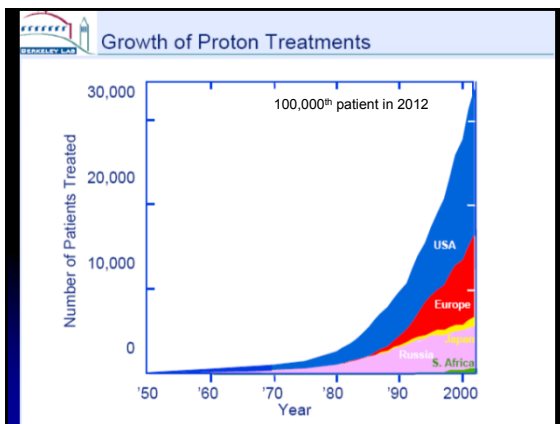
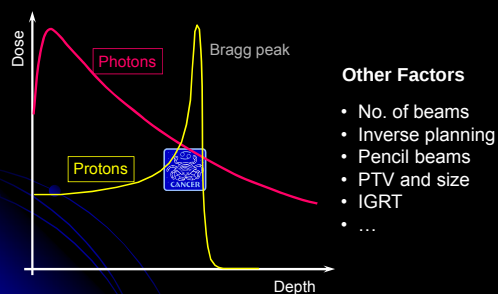
Scripps Proton Therapy Center



Goals

- Review proton therapy technologies and IMPT
- Compare differences between IMRT and IMPT
- Discuss challenges in using IMPT in clinical practice

Why protons?



Proton Therapy Centers in US



Tim Williams – Economics of Proton Therapy
ASTRO 2007 Proton Panel

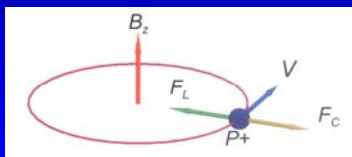
Reasons to Establish a Proton Center

- Belief in Clinical Efficacy
- Program Differentiator
- Revenue Generation
- Institutional Prestige
- Defensive Maneuver

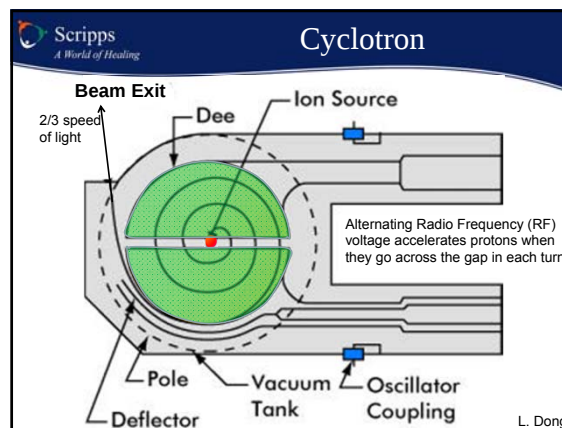
What are different proton systems?

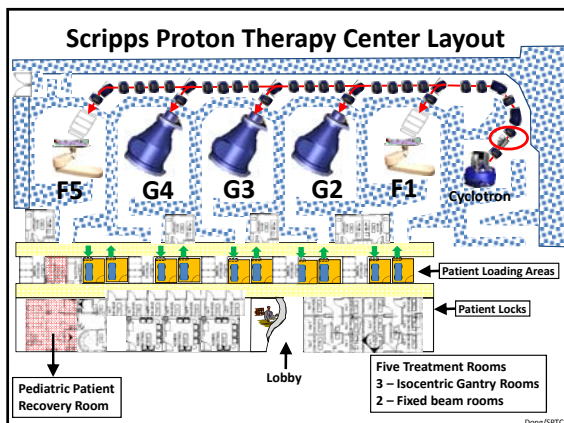
Physics

- Requires higher energy: 250 MeV p^+ ~ 30cm
- Requires magnetic field for beam acceleration and beam steering



Modified from
V. Jorgensen





Cyclotron

Cyclotron works while: T_{circle} independent from radius (particles move in pace with V_{dee})

However, at very strong magnetic fields:

Magnetic field decreases with radius

$\Rightarrow T_{\text{circle}}$ increases with radius
 $\Rightarrow$ particles lose pace with frequency of V_{dee} (RF).

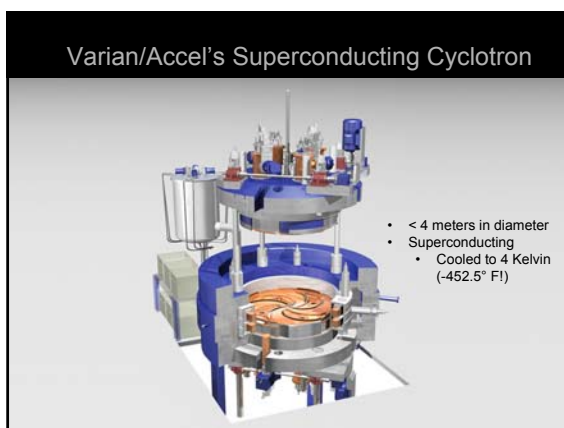
Remedy: decrease f_{RF} with radius:
synchro-cyclotron

$f_{\text{RF}} \sim 1 \text{ ms}$

$\Rightarrow$ pulsed beam (1 kHz)
 $\Rightarrow$ strong magnetic fields possible

$\Rightarrow$ Smaller machines !!

Novel Techniques in Accelerators and Gantry for Hadron Therapy | Marco Schepers, PSI | PT000 Edu Session Serial, May 15, 2012 | 15



Synchro-Cyclotron

8-10 T 250 MeV Synchro-cyclotron on a gantry

MEVION
medical systems

First beam extracted in May 2010

Novel Techniques in Accelerators and Gantry for Hadron Therapy | Marco Schepers, PSI | PT000 Edu Session Serial, May 15, 2012 | 16

Synchro-Cyclotron

8-10 T 250 MeV Synchro-cyclotron on a gantry

From Company data:

- dose rate: 2-4 Gy/min
- head leakage measured < 0.1% ($Q=10$)
- lateral penumbra $\approx$ conv. scatter systems

Beam analysis
 $\Rightarrow$ distal penumbra = 5.7 mm at all E

- scattering only
- pulsed beam $\Rightarrow$ scanning difficult
- \$ per treatment room > for multiroom facil.

Novel Techniques in Accelerators and Gantry for Hadron Therapy | Marco Schepers, PSI | PT000 Edu Session Serial, May 15, 2012 | 17

The Principle of Synchrotrons

Hitachi and Siemens Synchrotrons:

- Both designs use 7 MeV multi-turn injection for higher intensity: 1.2×10^{11} protons per pulse (Hitachi)
- Both use RF driven extraction for turning beam on and off quickly ($< 200 \mu\text{s}$) and for gated respiration
- Both are strong focusing with similar magnet layout and beam optical

LLUMC Synchrotron:

- Uses slow extraction with 0.2 – 0.5 sec every 2.2 sec
- weak focusing



Beam Delivery System

- Gantry
 - Position beam in different angles (isocentric)
 - Mounting of imaging systems
 - Lasers
- Fixed beam port (horizontal/inclined)
- Nozzle
 - Delivery the protons
 - Dose monitoring system
 - Beam shaping devices
 - Protect patient from unwanted radiation
 - Imaging (optional)



Multi-room Systems

- | | |
|---------------|--|
| • Hitachi | 270 MeV proton synchrotron |
| • IBA | 230MeV cyclotron |
| • Mitsubishi | 235 MeV proton synchrotron |
| • Mitsubishi* | 320MeV/u synchrotron (20 cm – ^{12}C) |
| • Optivus | 250 MeV proton synchrotron |
| • ProTom | 330 MeV/u proton synchrotron |
| • Siemens * | 430 MeV/u synchrotron (30 cm – ^{12}C) |
| • Varian | 250MeV superconducting cyclotron |

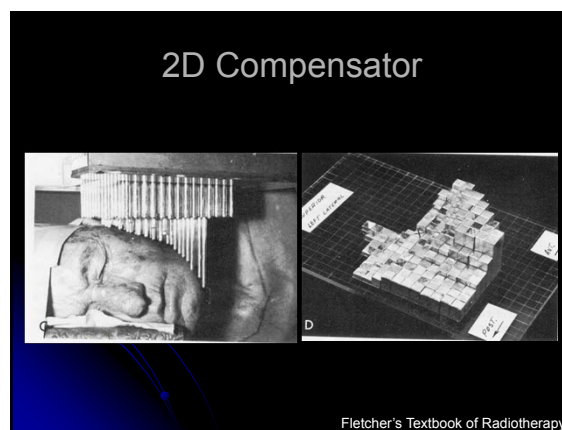
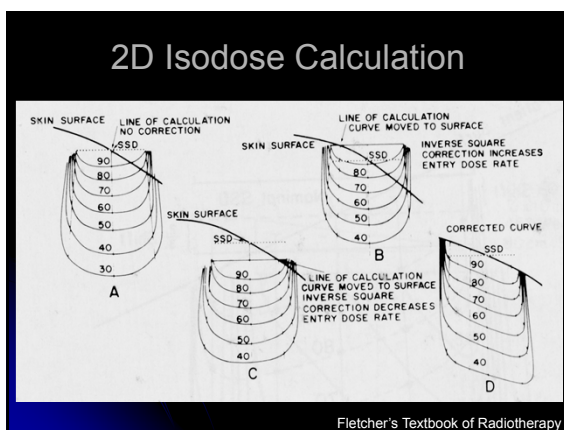
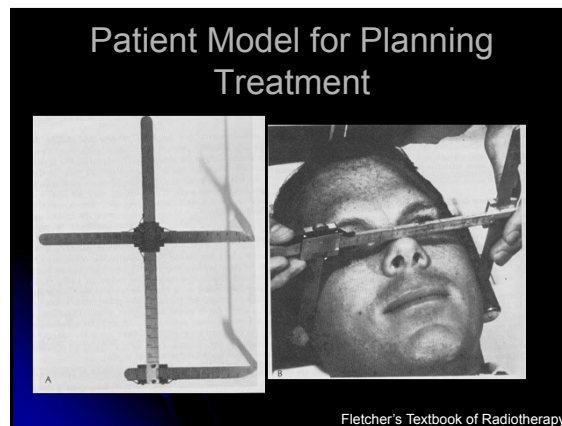
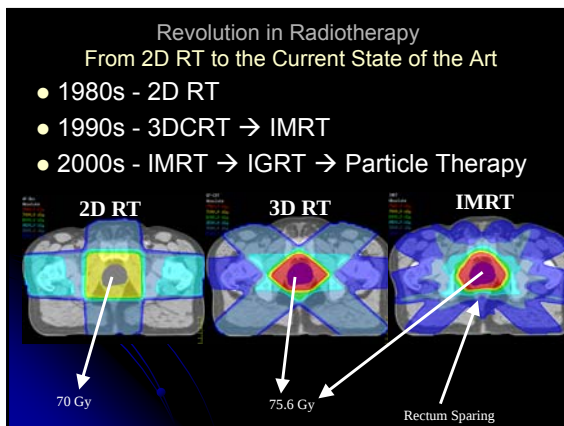
* Proton and ^{12}C

Single Room Systems

- | | |
|---------------|---|
| • Mevion: | 250 MeV gantry mounted compact superconducting synchrocyclotron. In production. |
| • IBA | ProteusOne |
| • Tomotherapy | 250 MeV Dielectric Wall Accelerator. Compact linear accelerator. Feasibility testing. |

From 2D to 3D

What have been changed?



What Is Intensity Modulated Radiation Therapy (IMRT)

An approach to deliver conformal therapy with optimized non-uniform beam intensities:

- Use computer mathematical scoring to design non-uniform radiation fields,
- Use dynamic motion of Multileaf Collimator to "paint" dose where desired - Intensity Patterns.

LD 01/02

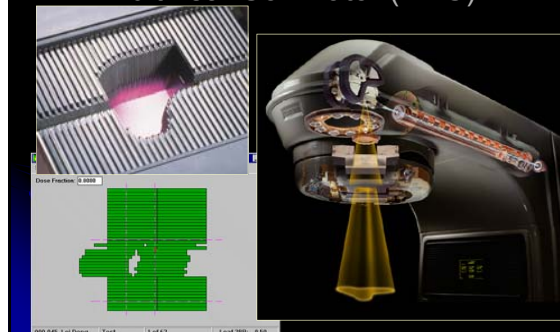


Why is IMRT Possible Today?

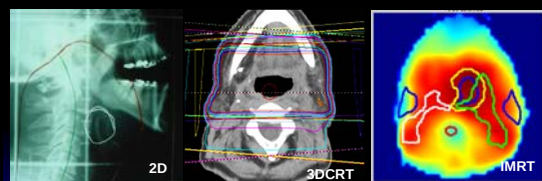
- Computer power sufficient to calculate plans in reasonable amount of time
- Linear Accelerators are computer - controlled
- Automated methods of machine setup and setup verification are convenient and commonplace
- Multileaf collimators have good mechanical precision and reliability

LD 03/03

Computerized Treatment System Multi-leaf Collimator (MLC)

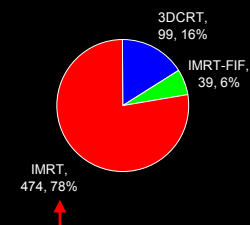


From 2D to 3D to IMRT



New H&N Cases at MDACC (2007)

- IMRT was the major treatment choice.
- 3DCRT: conventional RT
- FIF: manual field-in-field IMRT
- IMRT: computer-optimized IMRT

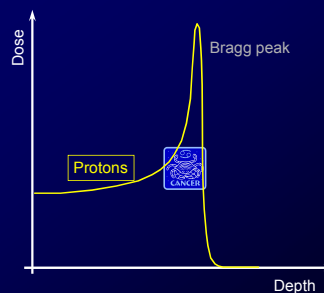


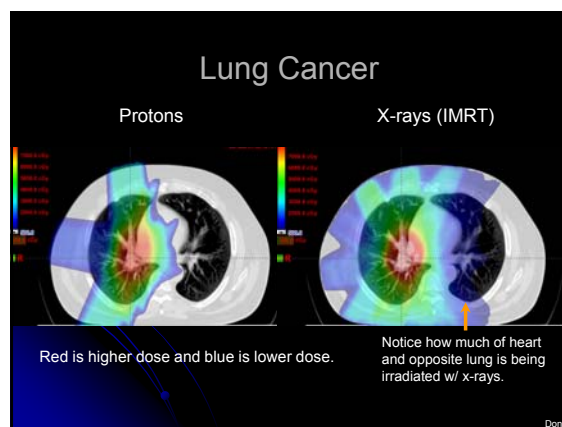
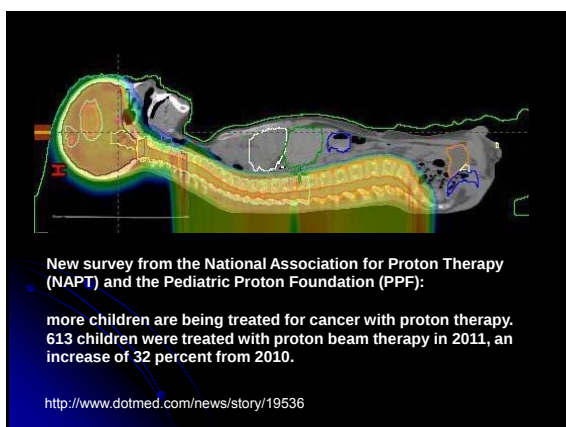
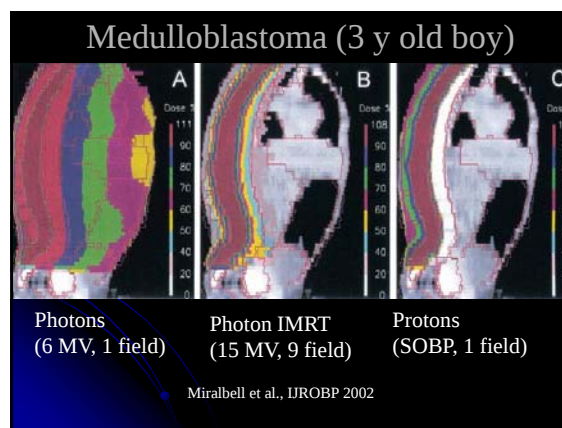
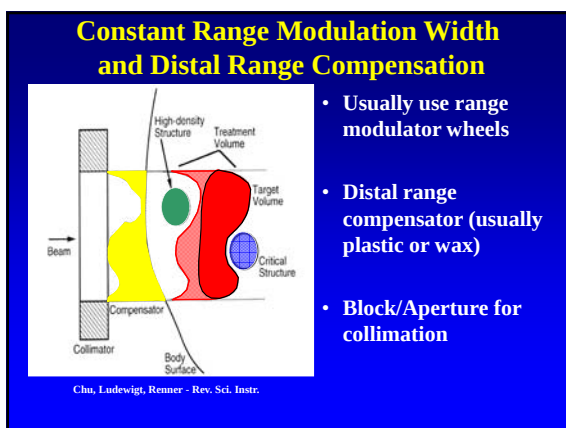
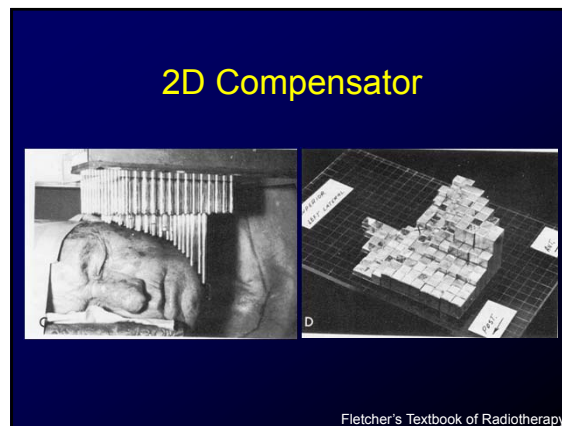
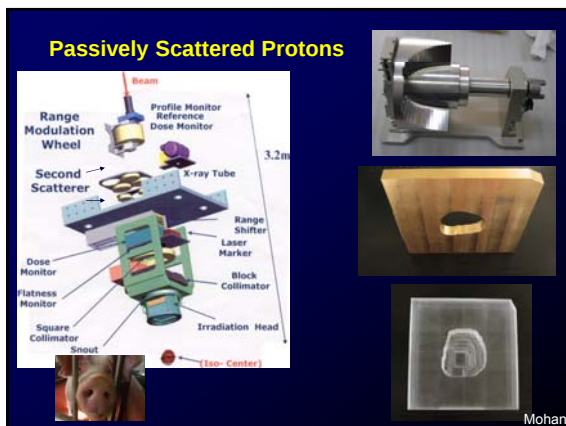
Lei Dong 2/29/2008

Technology Evolution in Proton Therapy

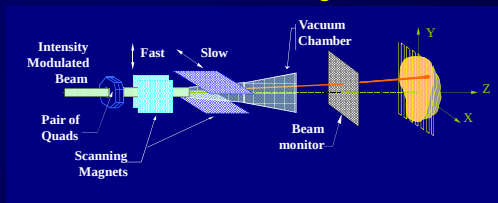
From Scatter to Scanning

Single Pencil Beam is insufficient for Treating Tumor



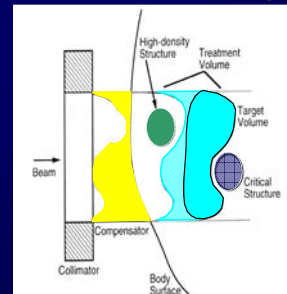


Pencil beam scanning nozzle



- Layer-by-layer scanning (changing energy is not easy)
- Spot scanning or raster scanning
- Max patient field (40x30) cm²

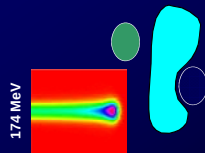
Constant Range Modulation Width and Distal Range Compensation



Chu, Ludewigt, Renner - Rev. Sci. Instr.

- Usually use range modulator wheels
- Distal range compensator (usually plastic or wax)
- Block/Aperture for collimation

Pencil Beam Scanning is Simpler



- Variable energy to treat tumor at different depth
- Dose conformity for both distal and proximal surfaces
- Sharp pencil beam to replace aperture

Why is PBS Possible Today?

- Better power supply for magnets (dipole; quadrupole; fast scanning coils)
- More advanced accelerator technology
 - More efficient accelerator
 - Better beam optics (smaller spots)
 - Fast energy change and current modulation
 - Automatic beam tuning and control system
- Scanning nozzle (~ MLC)

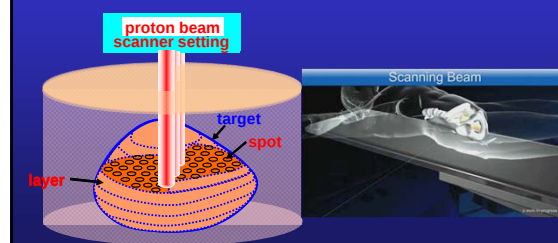
LD 04/13

Advantages for using Pencil Beam Scanning

- Fewer neutrons
- No physical compensator or aperture
- Sparing of healthy tissues proximal to the target
- Large treatment field
- Intensity and energy modulated proton therapy (IMPT)
 - Inverse planning
 - Dynamic dose painting (control points)

Step-and-shoot delivery of proton beam scanning

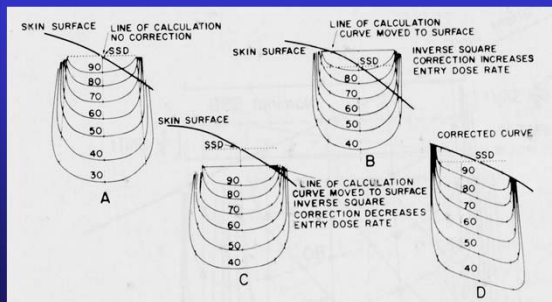
Discrete spot scanning method



Modified from Martin Bues, PhD.

From Varian

2D Isodose Calculation



Fletcher's Textbook of Radiotherapy

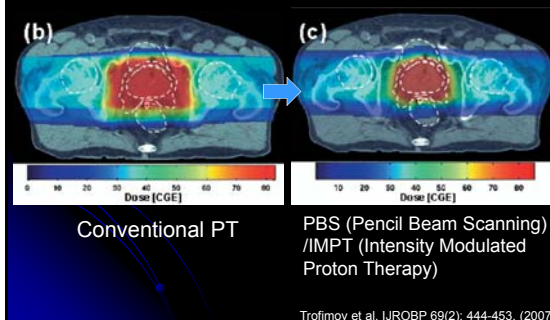
Proton Beam Delivery Mode

- Passive Scatter (PS)
 - Use scatter technique to create a large treatment field
 - Range modulation is required
- Uniform Scanning (US)
 - Pre-programmed PBS with beam aperture (more tolerant of motion)
- Pencil Beam Scanning (PBS)
 - Use magnetic field to scan the treatment field
 - High intensity modulation (better plans)
 - Energy (range) can be changed spot-by-spot

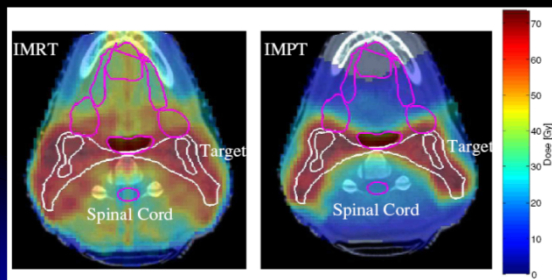
Raster Scan vs. Spot Scan

- Intensity modulation is much higher in spot scanning technique, which leads to better treatment plans
- Raster scanning may be more tolerant for organ motion

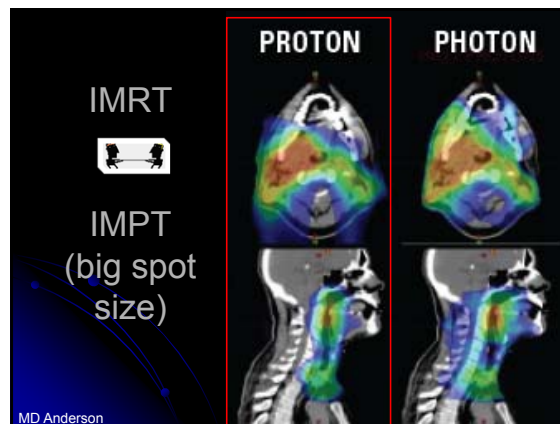
Evolution of Proton Therapy

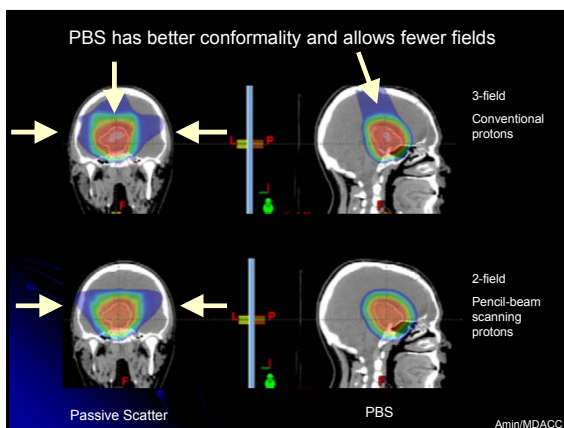


Photons vs. Future Protons



Bortfeld T. IMRT: "A review and a preview", Phys. Med. Biol. 51(13), 2006.





IMRT vs. IMPT

- IMPT typically use fewer beams
 - 2-3 (IMPT) vs. 5-9 (IMRT)
- Range uncertainties – PTV concept
 - Metal artifacts
 - Patient scatter
- Normal tissue motion is important
- IGRT
 - CBCT is lacking in proton therapy centers (today)

Image Guidance in New Systems



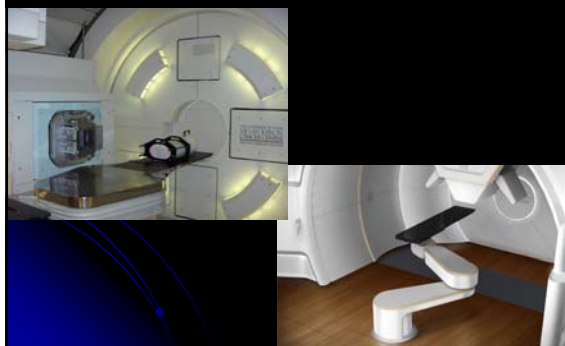
Image Guidance

- X-ray source to axis distance = 2 meters
- Detector to axis distance = 1 meter



Courtesy of Varian

Robotic Couch

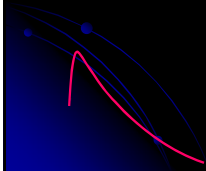


Challenges

Inverse Planning Challenges

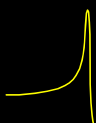
IMRT

- Beam angle
- Pencil beam position
- Pencil beam intensity



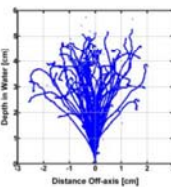
IMPT

- Beam angle
- Pencil beam position
- Pencil beam intensity
- Pencil beam energy
- Pencil beam spacing $f(E)$
- Robustness considerations

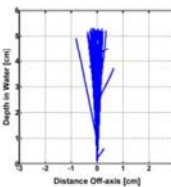


Straggling from Multiple Particle Paths

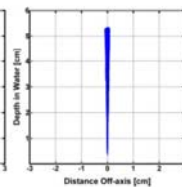
10 MeV electrons
50 histories



80 MeV protons
50 histories



150 MeV/n carbon ions
500 histories

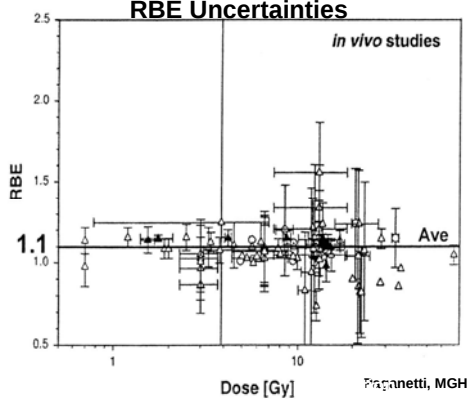


MCNPX simulations

Moyers
PTCOG 2010

RBE Uncertainties

in vivo studies

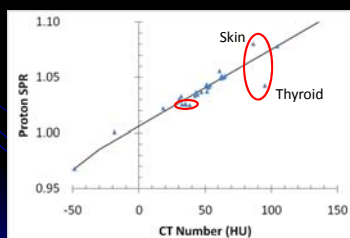


CT Number Uncertainties

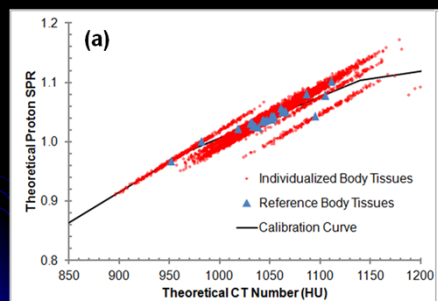
Leading to errors in predicted
proton range in patient

CT number to Proton Stopping Power

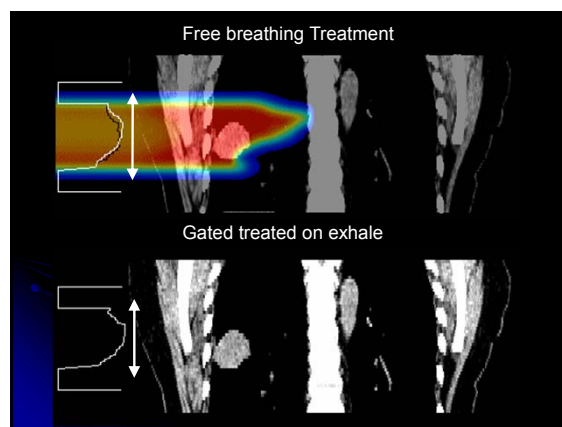
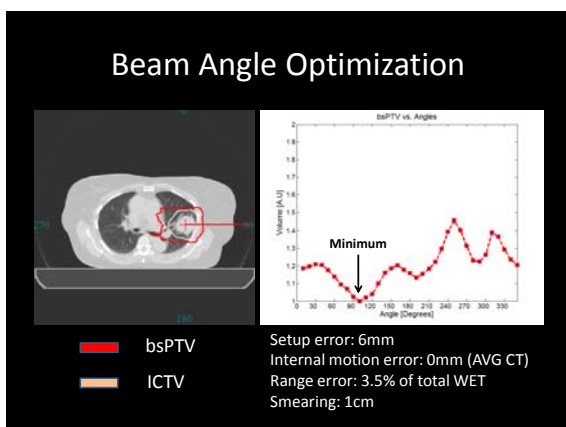
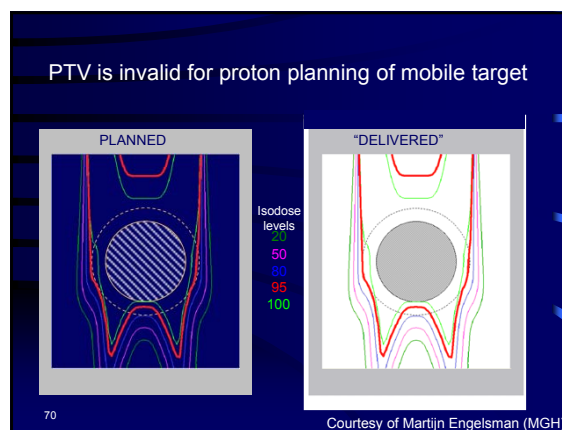
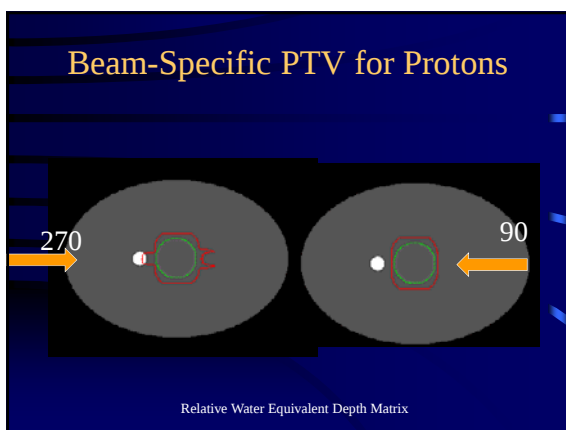
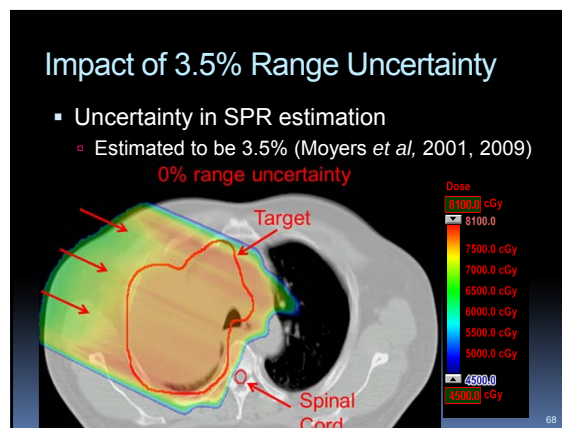
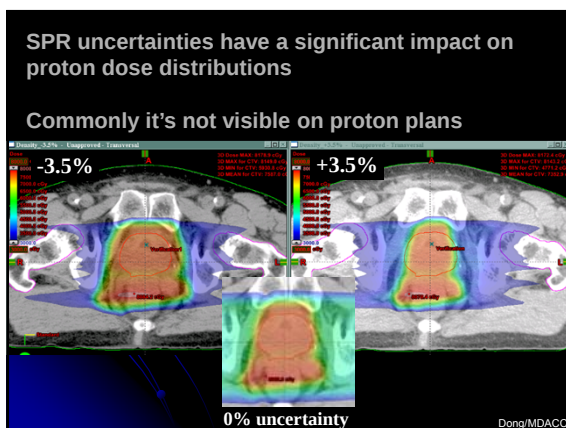
- Degeneracy problem
 - $HU(\rho_1, Z_1) = HU(\rho_2, Z_2)$
 - $SPR(\rho_1, Z_1) \neq SPR(\rho_2, Z_2)$

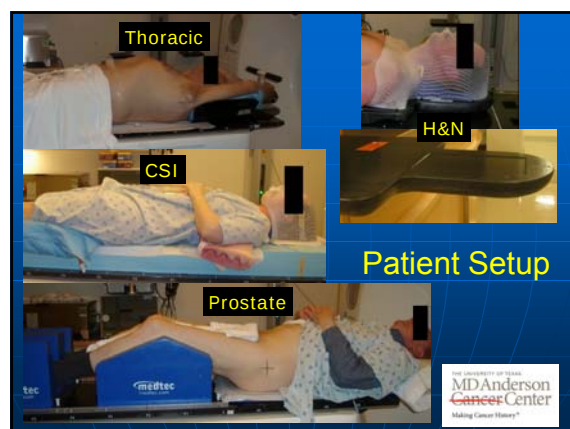
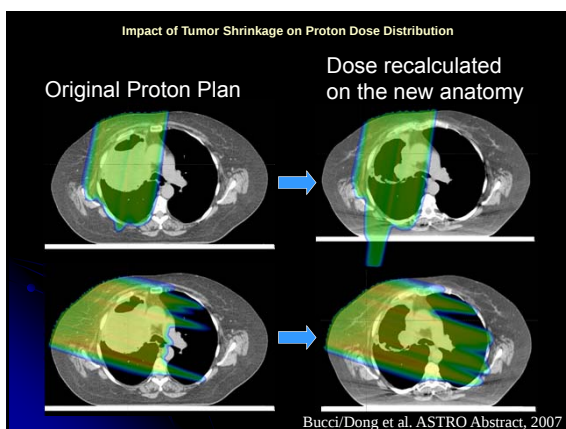
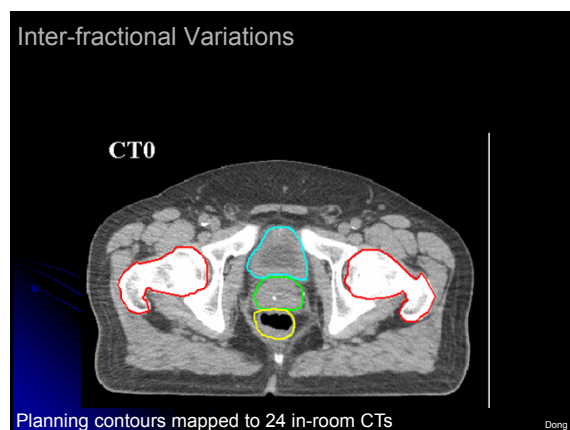
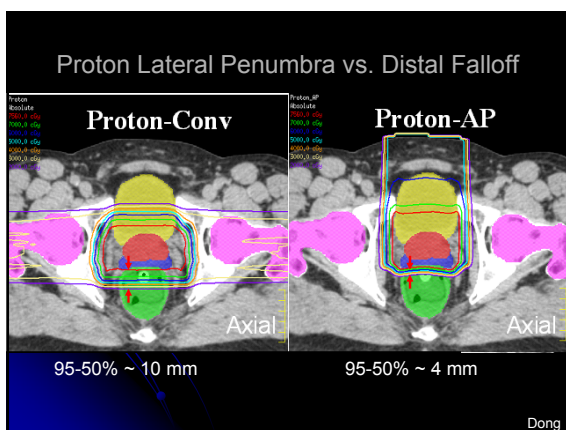
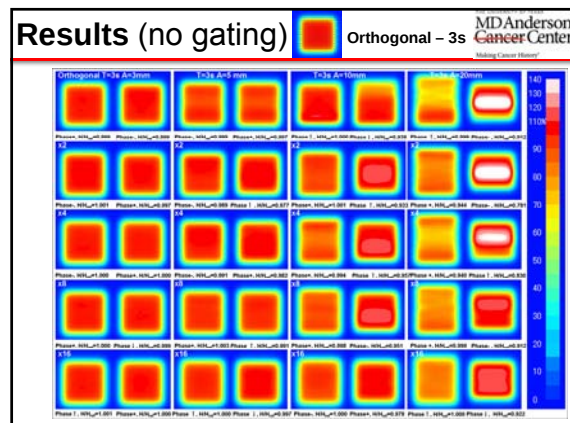
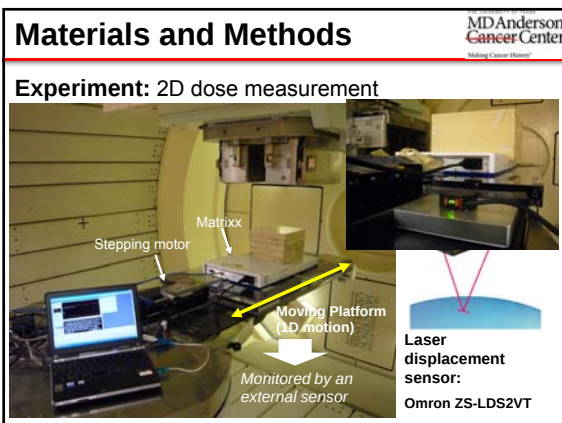


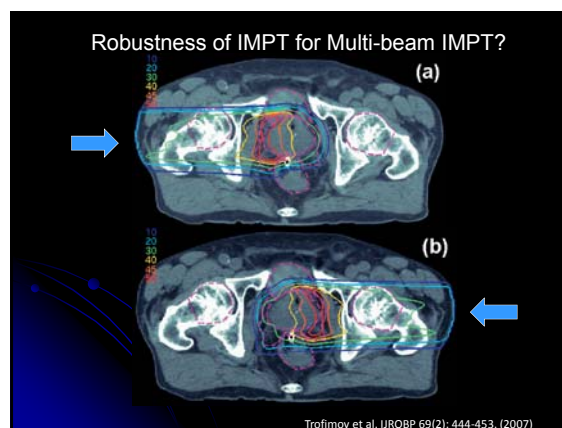
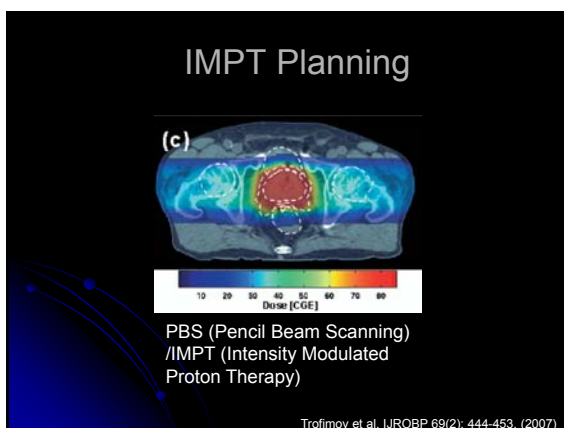
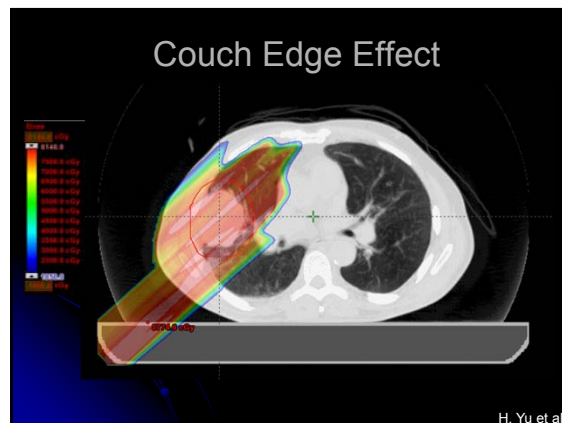
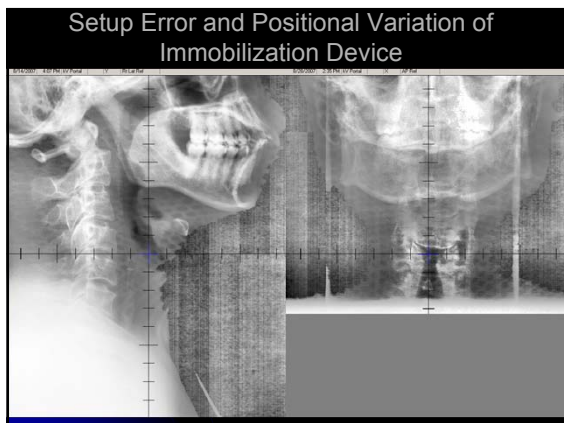
Variations in Human Tissue Composition



Yang M.

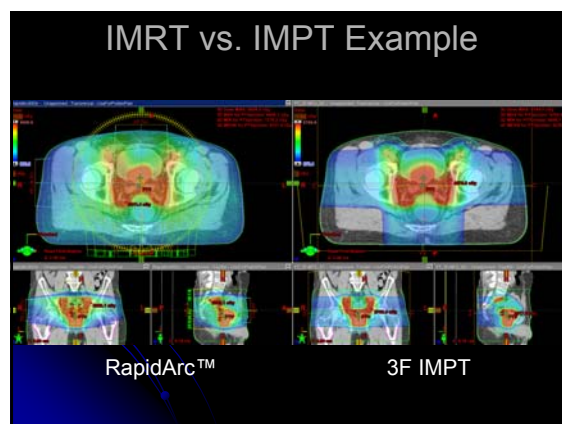


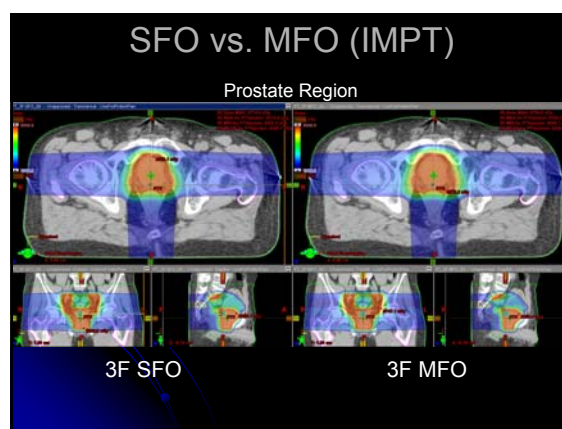
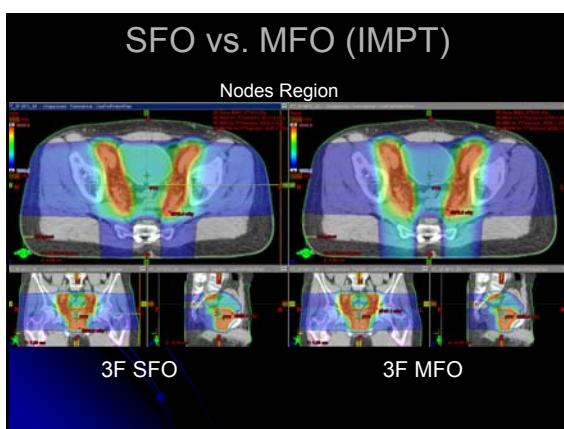
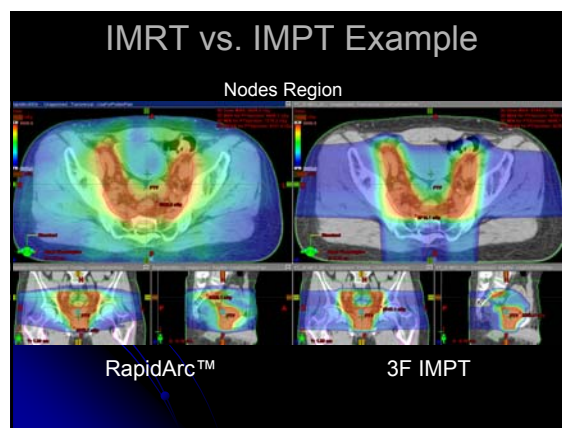
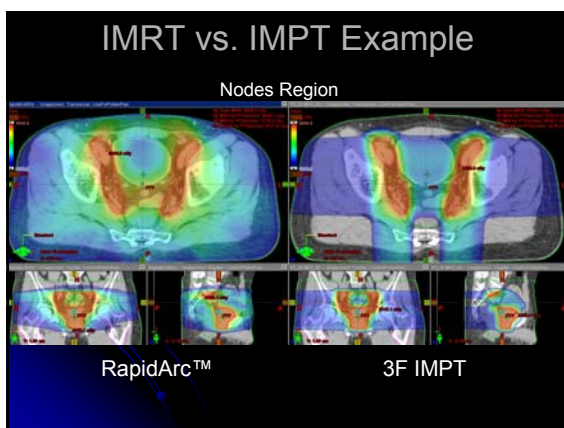
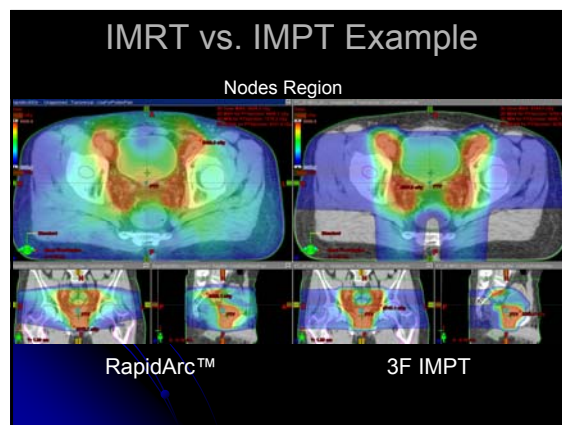
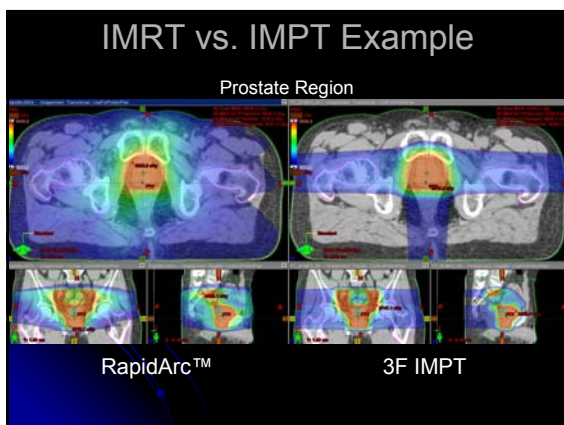


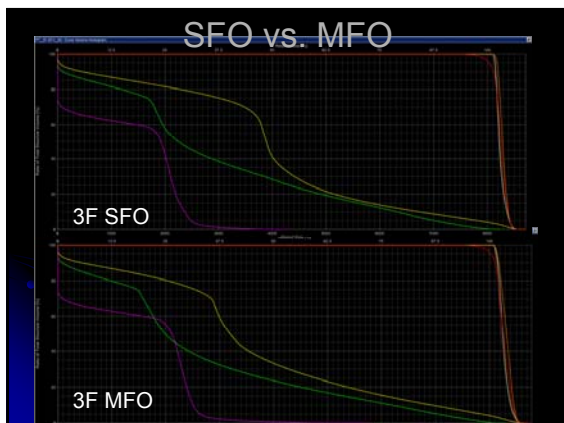


SFO vs. MFO

- Single-Field Optimization
 - Treat the entire target from one beam
 - Less normal tissue sparing
 - Relatively more robust for range uncertainties
- Multi-Field Optimization
 - Simultaneous optimization of multiple beams for one or more targets
 - Better plan (on paper) and more tissue sparing
 - Sensitive to range uncertainties and organ motion







Robustness Evaluation

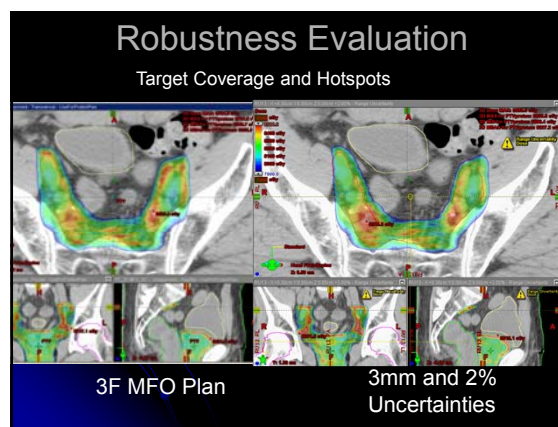
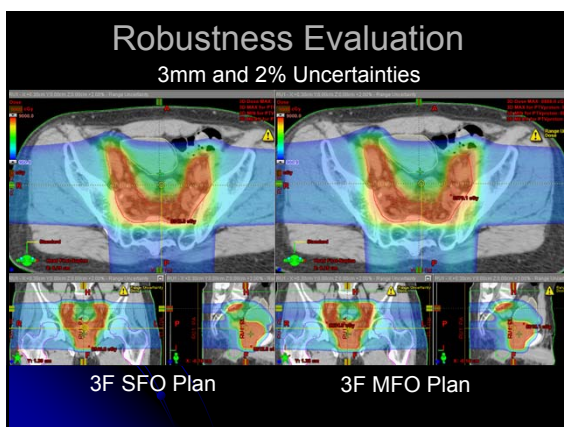
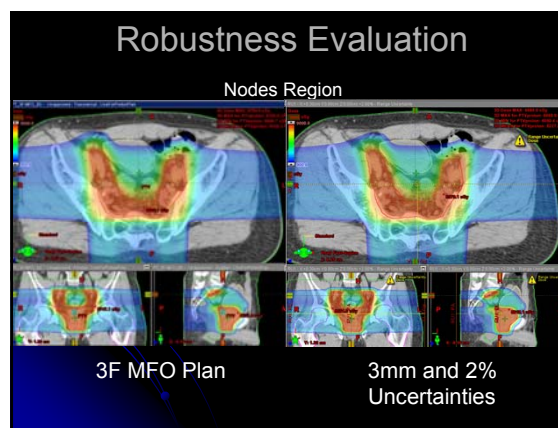
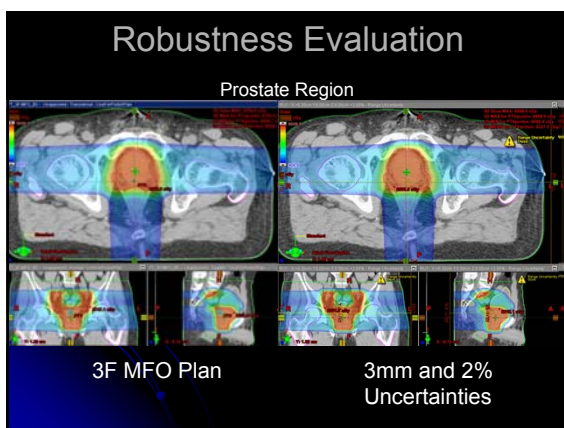
Range Uncertainty Parameter Organizer

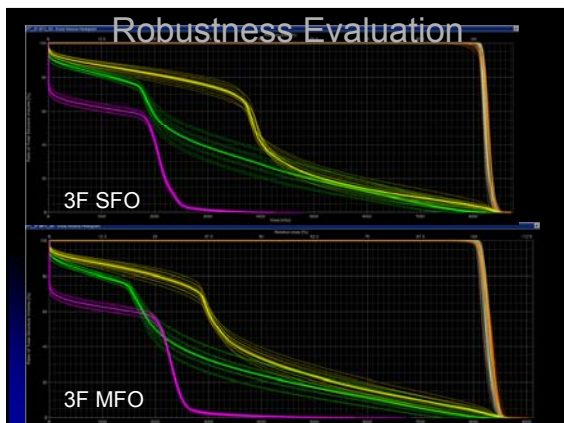
Generate Range Uncertainty Parameters

Isocenter shift [cm]: Calibration curve error [%]:

Range Uncertainty Parameters

ID	Δ	Isocenter shift			Curve Error [%]
		X [cm]	Y [cm]	Z [cm]	
RU1		+0.30	0.00	0.00	+2.00
RU2		+0.30	0.00	0.00	-2.00
RU3		-0.30	0.00	0.00	+2.00
RU4		-0.30	0.00	0.00	-2.00
RU5		0.00	+0.30	0.00	+2.00
RU6		0.00	+0.30	0.00	-2.00
RU7		0.00	-0.30	0.00	+2.00
RU8		0.00	-0.30	0.00	-2.00
RU9		0.00	0.00	+0.30	+2.00
RU10		0.00	0.00	+0.30	-2.00
RU11		0.00	0.00	-0.30	+2.00
RU12		0.00	0.00	-0.30	-2.00





Summary

Challenges

- Development and optimal use of IMPT
- Measurement dosimetry
- In vivo range verification
- Robustness plan evaluation
- Robust plan optimization
- Motion management strategies
- Dose-guided setup and adaptive RT
- Workflow optimization and efficiency
 - Auto-segmentation
 - Workflow assessment and optimization
 - Setup outside of treatment room

Opportunities

- Development and optimal use of IMPT
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Future Proton Therapy
Machines will be Different
from Today!

What is IMRT?

I'M Really Tired

What is IMPT?

I'M Painfully Tired